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### A High Power Buckypaper Biofuel Cell: Exploiting 1,10-Phenanthroline-5,6-dione with FAD-Dependent Dehydrogenase for Catalytically-Powerful Glucose Oxidation

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7 **(S)** Supporting Information

ABSTRACT: Enzymatic biofuel cells generate electrical energy 8 from renewable sources with high selectivity and environmental 9 benefits compared to lithium batteries and traditional fuel cells. 10 For enzymatic fuel cells to become competitive, major improve-11 ments in electrode design are required to enhance power density, 12 voltage output, and stability. Here we have developed a 13 freestanding paper biofuel cell comprising redox molecule 14 embedded multiwalled carbon nanotube papers for electrical 15 wiring of enzymes. The drop-coat and one-pot fabrication 16



methods provide flexibility and permit easy scalability of functionalized bioelectrodes via commercially available materials. Buckypaper functionalized with 1,10-phenanthroline-5,6-dione (PLQ) as an efficient electron mediator for fungal-derived FADdependent glucose dehydrogenase (FADGDH) shows very high steady-state current densities for glucose oxidation of  $I_{max} = 5.38$  $\pm 0.54$  mA cm<sup>-2</sup> at 0.15 V vs SCE at neutral pH. When coupled with a bioinspired protoporphyrin IX buckypaper cathode, the

resulting glucose/O<sub>2</sub> fuel cell delivered a power density of  $0.65 \pm 0.1 \text{ mW cm}^{-2}$  or  $24.1 \pm 4.7 \text{ mW cm}^{-3}$  at a cell voltage of 0.5 V,

- 22 limited by the cathode. Galvanostatic and current discharge experiments confirm robust short-term operational performance.
- 23 KEYWORDS: bioelectrocatalysis, biocatalyst, paper electrode, enzymatic, FAD-GDH, multicopper oxidases

### 24 INTRODUCTION

25 Enzymatic biofuels (EBFCs) convert chemical energy into 26 electrical energy under mild conditions from the oxidation of 27 organic fuels such as sugars and alcohols, coupled with the 28 reduction of oxygen using redox enzymes as bioelectrocata-29 lysts.<sup>1-3</sup> Biofuel cells offer several advantages over lithium 30 batteries and traditional fuel cells, including the use of 31 renewable, low-cost, and safe fuels from ecological sources 32 and operation at neutral pH and ambient temperature. 33 Furthermore, EBFCs can operate as membraneless fuel cells 34 owing to the high selectivity of enzymes. Particular attention of 35 biofuel cells over the past decade has been directed toward the 36 use of EBFCs as micropower sources which harvest energy 37 from biological fluids for implantable medical devices.<sup>4–7</sup> In 38 recent years, EBFCs have been successfully implanted in rats,<sup>4</sup> 39 lobsters,<sup>5</sup> and snails.<sup>6</sup> Application of EBFCs for portable and 40 wearable devices is more feasible and has enormous potential. 41 For example, epidermal and contact-lens biofuel cells which 42 harvest energy from sweat or tears using carbon nanotube 43 based electrodes have started to emerge.<sup>8-10</sup> Lightweight 44 biofuel cells with small form factors offer the prospect of self-45 powered chemical sensors with in situ detection and 46 remediation of toxic chemicals.<sup>11,12</sup>

47 Specific challenges in EBFC electrode design include the 48 development of electrodes which offer (i) stable immobilization 49 of enzymes and mediators with high loadings, (ii) efficient electron transfer between the active sites of enzymes and the 50 electrode, and (iii) fast mass transport and (iv) are lightweight 51 and easily integrated into devices. To achieve the practical 52 application of biofuel cells, a rapidly emerging approach is to 53 use flavin adenine dinucleotide-dependent glucose dehydrogen- 54 ase (FADGDH) for catalytic oxidation of glucose at the anode. 55 The FADGDH enzyme offers major advantages for biofuel cells 56 compared to other popular FAD-dependent enzymes such as 57 the gold standard glucose oxidase (GOx).<sup>13,14</sup> Unlike GOx, 58 FADGDH is oxygen insensitive, which prevents consumption 59 of valuable oxygen at the anode. In situ production of hydrogen 60 peroxide, which can be toxic to single compartment fuel cells, is 61 also avoided.<sup>14</sup> However, the commercially available fungal 62 FADGDH does not have the cytochrome-complex subunit for 63 direct electron transfer (DET) with electrodes.<sup>15</sup> As such, the 64 fungal FADGDH requires an artificial electron transfer 65 mediator, which can result in kinetic and thermodynamic 66 losses compared to DET.<sup>16</sup> The identification of high 67 performance mediators is vital for fungal FADGDH for both 68 biofuel cell and sensor applications. Few systems for mediated 69 electron transfer with FADGDH have been investigated and are 70 mainly based on osmium,<sup>13,17–19</sup> ruthenium,<sup>20</sup> and ferro- 71

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72 cene<sup>14,21</sup> redox complexes and polymers. These mediators have 73 high redox potentials and slow mediator exchange due to 74 structural rigidity and require complicated synthesis from toxic 75 precursors. Compared to metal-based mediators, small organic 76 mediators with fast mediator exchange are attractive. For 77 example, 1,2 and 1,4 naphthoquinones<sup>22,23</sup> and phenothia-78 zines<sup>24,25</sup> are commonly exploited and give high catalytic 79 currents at attractively low formal redox potentials.

80 Carbon nanotubes (CNTs) offer great advantages for 81 bioelectrodes and are typically deposited onto an electrode 82 support to give a large surface area with good stability and 83 conductivity.<sup>26</sup> CNT-supported electrodes tend to be heavy, 84 bulky, and not easily miniaturizable.<sup>27,28</sup> Free-standing bucky-85 paper electrodes prepared by vacuum filtration of CNT 86 suspensions on the other hand are thin and lightweight and 87 offer the possibility to immobilize catalysis-promoting aromatic 88 molecules by π-stacking interactions.<sup>29–32</sup> However, such paper 89 electrodes are often fragile with limited conductivity and slow 90 electron transfer kinetics compared to conventional bulk 91 electrodes such as glassy carbon (GC). Further improvements 92 in fabrication methods are required toward CNT paper 93 electrodes with excellent homogeneity, reproducibility, and 94 electrochemical properties.

In this study, we report the preparation of new redox 95 96 molecule embedded buckypapers for bioelectrocatalysis using 97 four different types of commercially available redox molecules. 98 The focus of the study is the development of high performance 99 catalytic buckypaper bioelectrodes for enzyme wiring without 100 the use of a supporting substrate or polymer scaffold. The use 101 of 1,10-phenanthroline-5,6-dione (PLQ) as a small electron 102 mediator for the fungus-derived FADGDH is explored, and the 103 resulting buckypaper anode integrated into a fully freestanding 104 paper glucose/O<sub>2</sub> biofuel cell with a protoporphyrin bucky-105 paper cathode. Notably, our approach here uses PLQ as a small 106 organic mediator and nanotube binder and therefore avoids 107 polymer and metal complex synthesis. This is in contrast to the 108 structurally and electronically different Ru polymer mediator 109 with PLQ ligands reported previously.<sup>20</sup>

### 110 **EXPERIMENTAL SECTION**

Materials and Apparatus. Monosodium phosphate 111 112 monohydrate (NaH<sub>2</sub>PO<sub>4</sub>, ≥98%), disodium hydrogen phos-113 phate heptahydrate (Na<sub>2</sub>HPO<sub>4</sub>, 98-102%), N,N-dimethylfor-114 mamide (DMF, 99.9%), potassium ferricyanide, 1,10-phenan-115 throline-5,6-dione (PLQ, 97%), protoporphyrin IX (PP,  $\geq$ 95%, 116 ferriprotoporphyrin IX (FePP, ≥98.0%), 1,4 naphthoquinone 117 (NQ, 97%), potassium chloride (KCl, 99%), D-(+)-glucose (≥99.5%), sodium citrate (>99%), sodium chloride (NaCl, 118 119 99.8%), copper chloride (CuCl<sub>2</sub>, 97%), hydrogen peroxide  $(H_2O_2, 30 \text{ wt } \% \text{ in } H_2O)$ , ethylenediaminetetraacetic acid 120 121 (EDTA, 99%), and sulfuric acid (95-98%) were purchased 122 from Sigma-Aldrich and used as received. Bilirubin oxidase 123 (BOD, 1.2 U mg<sup>-1</sup>) from Myrothecium sp. and flavin adenine 124 dinucleotide-dependent glucose dehydrogenase (FADGDH, 125 1150 U mg<sup>-1</sup> solid) from Aspergillus sp. were purchased from 126 Amano (Japan) and Sekisui Diagnostics (UK), respectively, and 127 used as received. Enzymes were stored at -20 °C. Distilled water was obtained by water purification to a resistivity of 15 128 129 M $\Omega$  cm using a Millipore Ultrapure system. Commercial grade 130 multiwalled carbon nanotubes (MWCNTs,  $\emptyset = 9.5$  nm, 1.5  $\mu$ m 131 length,  $\geq$ 95% purity) were obtained from Nanocyl and used as 132 received without purification. High purity oxygen and argon

were obtained from Messer. Glucose solutions were left to 133 mutarotate overnight to  $\beta$ -D-glucose prior to use. 134

Preparation of Unmodified MWCNT Buckypaper and 135 Redox-Embedded MWCNT Buckypaper Electrodes by 136 Drop-Coat Method. First, a 1 mg mL<sup>-1</sup> MWCNT suspension 137 was prepared by the addition of 150 mg of nonfunctionalized 138 MWCNTs into 150 mL of DMF. The dispersion was then 139 sonicated for 30 min prior to use. After vigorous shaking for 1 140 min, 66 mL of the suspension was filtered through a Millipore 141 PTFE filter (JHWP, 0.45  $\mu$ m pore size, Ø = 46 mm) using a 142 vacuum pump, washed with distilled water, and left for 1 h. 143 After filtration, the resulting unmodified buckypaper with  $\emptyset = 144$ 35 mm was left to dry at room temperature. The buckypaper 145 was obtained after its careful removal from the filter paper, then 146 cut into individual electrodes with  $\emptyset = 10 \text{ mm}$  (geometric 147 surface area of 0.785 cm<sup>-2</sup>) using a metal cutter. To obtain 148 functionalized MWCNT buckypaper electrodes, 150 µL of 0.6 149 mmol L<sup>-1</sup> or 10 mmol L<sup>-1</sup> modifier (PP and FePP) in DMF 150 was drop-coated onto unmodified buckypaper surfaces with Ø  $_{151}$ = 10 mm (each electrode contains 5.39 mg of MWCNTs) and 152 the resulting electrode left to dry overnight at room 153 temperature. Electrical contact was obtained via a metal wire 154 with carbon paste. The back and sides of the electrode were 155 sealed with silicone paste. 156

Preparation of Redox-Embedded MWCNT Bucky- 157 paper Electrodes by One-Pot Method. A 1 mg mL<sup>-1</sup> 158 MWCNT suspension was first prepared by the addition of 150 159 mg of nonfunctionalized MWCNTs into 150 mL of DMF. The 160 dispersion was then sonicated for 30 min prior to addition of 161 the modifier (PLQ, NQ, PP, and FePP). The modifier, 162 dissolved in a minimum volume of DMF, was slowly added 163 into the MWCNT suspension to give a final 0.6 mmol  $L^{-1}$  or 2 164 mmol L<sup>-1</sup> modifier concentration. Prior to filtration, the 165 resulting suspension was sonicated for a further 30 min. After 166 rigorous shaking for 1 min, 66 mL of the suspension was 167 filtered, washed, and dried (as above for the unmodified 168 buckypaper) and the resulting buckypaper cut into electrodes 169 with  $\emptyset = 10$  mm. Electrical contact was obtained via a metal 170 wire with carbon paste. The back and sides of the electrode 171 were sealed with silicone paste. 172

**Preparation of Buckypaper Bioelectrodes.** First, 5 mg 173 mL<sup>-1</sup> stock solutions of BOD and FADGDH were prepared in 174 0.1 mol L<sup>-1</sup> phosphate buffer at pH 7.0 and McIlvaine buffer at 175 pH 7.0 (0.2 mol L<sup>-1</sup> Na<sub>2</sub>HPO<sub>4</sub>, 0.1 mol L<sup>-1</sup> citric acid), 176 respectively. A total of 150  $\mu$ L of 5 mg mL<sup>-1</sup> enzyme solution 177 (0.75 mg enzyme) was then added to the surface of a 178 buckypaper with  $\emptyset$  = 10 mm, and the enzyme solution was 179 allowed to fully absorb at 4 °C overnight. The electrode was 180 subsequently rinsed with the corresponding buffer before use. 181

**Electrochemistry.** Electrochemical measurements were 182 performed at room temperature using an Eco Chemie Autolab 183 PGSTAT 100 potentiostat running GPES 4.9 software or a 184 Biologic VMP3Multi Potentiostat with EC-lab software. For 185 half-cell testing, a conventional three-electrode cell setup was 186 used comprising a buckypaper working electrode ( $\emptyset = 10 \text{ mm}$ ), 187 a saturated calomel reference electrode (SCE with sat. KCl), 188 and a Pt wire counter-electrode. The complete fuel cell setup 189 comprised a one-pot protoporphyrin buckypaper with BOD 190 biocathode (BP<sub>PP</sub>-BOD) and a one-pot phenanthroline 191 quinone buckypaper with FADGDH (BP<sub>PLQ</sub>-FADGDH) 192 bioanode immersed in 20 mL of McIlvaine buffer at pH 7.0 193 with an interelectrode distance of 3 mm. Gas flows were set 194 qualitatively and moderately to obtain reproducible conditions. 195 196 Average catalytic current densities were obtained by subtracting 197 the background current: the signal obtained without oxygen, for 198 the cathode, and without glucose, for the anode. Fuel cell 199 experiments were performed by recording a linear sweep 200 polarization from the open circuit voltage (OCV) to 0.02 V 201 with the anode connected to the counter and reference leads, 202 and the cathode connected to the working lead. Power densities 203 were obtained by dividing the power delivery by the surface 204 area or volume of one electrode.

**Scanning Electron Microscopy.** Buckypaper electrodes with  $\emptyset = 3$  mm were imaged using a FEI/Quanta FEG 250 zor scanning electron microscope (Hillsboro, OR, USA) operating at an accelerating voltage of 5 kV without metal coating.

**Static Water Contact Angles.** Water contact angles were 210 obtained at room temperature by delivering a 2  $\mu$ L droplet of 211 distilled water onto the sample surface on a horizontal stage 212 using a Dataphysics OCA 35 system. Multiple droplet 213 measurements (8 or 9) were recorded per sample type.

### 214 **RESULTS AND DISCUSSION**

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Characterization of Unmodified MWCNT and Redox-215 216 Embedded MWCNT Buckypaper Electrodes. Pristine freestanding buckypaper prepared from filtration of CNT 217 dispersions without additives tends to be fragile and difficult to 218 manipulate. Our initial experiments established that the ability 219 to handle pristine unmodified BP was improved when the 220 amount of MWCNTs in the final product was increased by at 221 least a factor of 2.30 Redox-embedded BP was subsequently 222 prepared in several steps (see Experimental Section) either by 223 the addition of redox molecules to the MWCNTs dispersion 224 before filtration (one-pot method) or after filtration by drop-225 coating onto the unmodified BP (drop-coat method). The BP 226 functionalization is based on  $\pi - \pi$  stacking interactions between 227 aromatic groups and CNT sidewalls. For all buckypapers, flat 228 229 and reproducible disks were obtained after filtration (Figure 230 1A), drying, and cutting (Figure 1B and C, respectively). BP thicknesses ranged between 230 and 320  $\mu$ m (see Table S1). 231 232 The variability in thickness results from differences in vacuum 233 pressure and the MWCNTs dispersion.

Scanning electron microscopy was performed to evaluate the 234 235 morphology of unmodified BP (BP, Figure 1D) and BP prepared from the one-pot method with redox molecules: 236 protoporphyrin IX (BP<sub>PP</sub>, Figure 1E), ferriprotoporphyrin IX 237 BP<sub>FePP</sub>, Figure 1F), and 1,10-phenanthroline-5,6-dione 238 (BP<sub>PLO</sub>, Figure 1G). The SEM images reveal that the BPs 239 comprise a random and entangled network of MWCNTs with 240 nanoscale porosity. The images show subtle evidence that 241 functionalized BPs have a flatter and more compact topography 242 compared to unmodified BP, suggestive of more intimate 243 interactions between nanotubes in the presence of redox 244 molecules via  $\pi - \pi$  stacking. 245

Cyclic voltammograms (CVs) of the  $Fe(CN)_6^{3-}$  redox probe 246 recorded at unmodified and BP<sub>PP</sub> paper electrodes reveal a 247 significant increase in peak current with a decrease in peak-to-248 peak separation  $(\Delta E_{\rm p})$  following modification with proto-249 250 porphyin molecules (see Figure S1). The dramatic enhance-251 ment with chemical functionalization is partially attributed to a physical improvement in the electronic connectivity between 252 253 carbon nanotubes. The increase in peak current observed is also 254 partially attributed to improved diffusion of  $Fe(CN)_6^{3-/4-}$  in 255 the 3D-structured electrode, facilitated by the increased surface 256 hydrophilicity (Figure S2).



**Figure 1.** (A, B) Photographs of freshly prepared  $BP_{PP}$  buckypaper (A) after filtration and (B) after filtration, drying, and cutting into the electrode. (C–G) SEM micrographs of (C, E)  $BP_{PP}$ , (D) BP, (F)  $BP_{FePP}$ , and (G)  $BP_{PLQ}$  buckypaper electrodes recorded at (C) 60×, (D–G) 5000× and 40 000× (inset) magnification. All modified electrodes were prepared by the one-pot method.

To investigate the presence and accessibility of porphyrin 257 and PLQ molecules in BP prepared via the one-pot and drop- 258 coat methods, cyclic voltammetry was performed on one-sided 259 BP samples with a geometric surface area of 0.785 cm<sup>2</sup>. CVs 260 were first recorded at functionalized electrodes prepared by the 261 one-pot method in argon-saturated 0.1 mol L<sup>-1</sup> phosphate 262 buffer at pH 7.0. Figure 2 shows CVs recorded at BP<sub>FePP</sub> and 263 f2 BP<sub>PLQ</sub> prepared via the one-pot method. The CVs reveal the 264 presence of well-defined chemically reversible processes. At 265 BP<sub>FePP</sub>, the one-electron Fe<sup>III</sup>/Fe<sup>II</sup> redox couple is observed at 266  $E_{1/2} = -0.38$  V vs SCE (10 mV s<sup>-1</sup>), consistent with reported 267



Figure 2. (A,B) CVs recorded at (A)  $BP_{FePP}$  and (B)  $BP_{PLQ}$  buckypaper electrodes (one-pot method) in Ar saturated 0.1 mol  $L^{-1}$  phosphate buffer at pH 7 at different scan rates. (C, D) Corresponding plots of anodic and cathodic peak current versus scan rate.

buckypaper electrode (number <sup>a</sup> )	fabrication method	modifier concentration (mmol $L^{-1}$ )	surface concentration <sup>b</sup> $(10^{-7} \text{ mol cm}^{-2})$	$\Delta E_{\rm p}~({\rm mV})$	$E_{1/2}$ (V)
$BP_{FePP} (n = 3)$	one-pot	0.6	$1.38 \pm 0.58$	65	-0.37
$BP_{FePP} (n = 3)$	drop-coat	0.6	$0.48 \pm 0.25$	55	-0.35
$BP_{FePP}$ $(n = 7)$	drop-coat	10	$6.43 \pm 3.58$	215	-0.36
$\mathrm{BP}_{\mathrm{PLQ}} \ (n=3)$	one-pot	2	$1.21 \pm 0.30$	118	-0.13
<sup><i>a</i></sup> Number of independent bucky mVs <sup>-1</sup> in Ar	ypaper electrode sar	nples analyzed. <sup>b</sup> Surface concentra	tions obtained from the anodic peak o	f CVs record	ded at 10

# Table 1. Electrochemical Parameters for $BP_{FePP}$ and $BP_{PLQ}$ Electrodes Prepared by One-Pot and Drop-Coating Functionalization Methods

268 values of  $E_{1/2} = -0.34$  V and -0.39 V vs SCE for FePP 269 modified MWCNTs on GC.<sup>33,34</sup> At BP<sub>PLQ</sub>, the two-electron 270 two-proton o-quinone/o-hydroquinone system is observed at 271  $E_{1/2} = -0.13$  V vs SCE (10 mV s<sup>-1</sup>) as previously observed for 272 PLQ adsorbed on MWCNTs on GC electrodes.<sup>35</sup>

Well-defined voltammograms and a linear dependence ( $r^2 > 274$  0.95) of peak current on scan rate for anodic and cathodic peaks are observed at the BP<sub>FePP</sub> and BP<sub>PLQ</sub> electrodes (Figure 276 2C and D), confirming that the redox molecules are accessible 277 and surface bound. The stability of the immobilized molecules 278 was tested by subjecting the electrodes to repeat potential 279 cycling at 20 mV s<sup>-1</sup> (Figure S3). No noticeable loss in 280 electroactivity was observed after 20 cycles, confirming the high 281 stability of the immobilized redox groups and the bulk 282 nanotube structure despite the noncovalent modification 283 approach.

Modified BP<sub>FePP</sub> electrodes prepared by the drop-coat method were also examined by voltammetry and gave the expected electroactivity as observed for the one-pot method. BP<sub>FePP</sub> electrodes were prepared by drop-coating 150  $\mu$ L of 0.6 mmol L<sup>-1</sup> or 10 mmol L<sup>-1</sup> FePP DMF solutions onto pristine unmodified BPs ( $\emptyset = 10$  mm). The electrochemical parameters obtained from CVs recorded in phosphate buffer at pH 7.0 and 291 10 mV s<sup>-1</sup> are listed in Table 1.

Examination of the data in Table 1 reveals that one-pot 292 293 BP<sub>FePP</sub> exhibits a higher surface concentration than drop-coat 294 BP<sub>FePP</sub>  $(1.38 \pm 0.58 \text{ versus } 0.48 \pm 0.25 \times 10^{-7} \text{ mol cm}^{-2})$  when 295 the same initial modifier concentration is used, consistent with 296 effective bulk functionalization via the one-pot method. <sup>297</sup> Increasing the modifier concentration from 0.6 mmol  $L^{-1}$  to 298 10 mmol  $L^{-1}$  resulted in a very high surface concentration of 299 6.43  $\pm$  3.58  $\times$  10<sup>-7</sup> mol cm<sup>-2</sup>, highlighting the possibility to 300 tailor redox molecule loading in the paper electrodes. It is 301 expected that such high surface concentrations would be 302 possible via the one-pot method with a 10 mmol  $L^{-1}$  modifier 303 concentration. However, this was not explored due to the high 304 volumes and quantity of modifier required for one-pot 305 buckypaper fabrication. The surface concentrations for FePP 306 prepared here are significantly higher than previously reported  $_{307}^{10}$  values of 6.8 × 10<sup>-10</sup> mol cm<sup>-2</sup> and 1.1 × 10<sup>-9</sup> mol cm<sup>-2</sup> for 308 FePP modified MWCNTs on GC.<sup>33,34</sup> The high loadings 309 observed here are consistent with an effective high surface area 310 3D-structured matrix.

Table 1 also reveals that  $BP_{FePP}$  prepared via one-pot and trop-coat methods with 0.6 mmol  $L^{-1}$  modifier solution give similar peak-to-peak separation values of  $\leq 65$  mV and therefore sits aimilar apparent electron transfer kinetics. Significantly larger therefore sluggish electron transfer kinetics  $\Delta E_p$  values and therefore sluggish electron transfer kinetics were observed for highly functionalized  $BP_{FePP}$  electrodes prepared with 10 mmol  $L^{-1}$  of the modifier. This is consistent with an extensive network of redox molecules being deeply embedded in the CNT structure, which would increase electron 319 tunneling distances and film resistivity. 320

On the basis of the BP<sub>FePP</sub> optimization experiments, we 321 prepared PLQ buckypaper via the one-pot method using a 322 modestly high concentration of 2 mmol L<sup>-1</sup>. No further 323 optimization was performed. The surface concentration 324 obtained for one-pot BP<sub>PLQ</sub> was  $1.21 \pm 0.30 \times 10^{-7}$  mol 325 cm<sup>-2</sup>, which reveals the possibility to obtain high redox 326 molecule loadings with a near  $1 \times 10^{-7}$  mol cm<sup>-2</sup> 327 concentration. The  $\Delta E_P$  value of 118 mV observed for BP<sub>PLQ</sub> 328 is consistent with a slow rate of electron transfer, increased BP 329 resistivity, and a large degree of potential inversion for the two-300 electron two-proton quinone process.<sup>36</sup>

Bioelectrocatalytic O2 Reduction at BPpp Electrodes 332 with Immobilized BOD Enzyme from Myrothecium 333 verrucaria. For biocathode construction, the multicopper 334 oxidase (MCO) enzyme BOD from Myrothecium verrucaria 335  $(M\nu)$  was employed as the catalyst for the four-electron 336 reduction of O<sub>2</sub> to H<sub>2</sub>O. BOD is a promising enzyme for 337 biofuel cells due to its high bioelectrocatalytic activity under 338 mild conditions and formal potential close to that of the O2/ 339  $H_2O$  couple (0.816 V vs RHE at pH 0). Bilirubin, as a natural 340 substrate for BOD, and its analogues, have been attached to 341 MWCNT electrodes to facilitate DET with  $M\nu$ BOD for O<sub>2</sub> 342 reduction.<sup>34,37</sup> The interaction is supported by favorable 343 immobilization and orientation. However, a commonly 344 accepted problem with BOD is that significant catalytic activity 345 loss is observed in the presence of  $H_2O_2$ , a common byproduct 346 of oxidase enzymes found in glucose/ $O_2$  biofuel cells. The use 347 of O2-insensitive FADGDH in biofuel cell design can 348 circumvent this issue. 349

In this study, the porphyrin-BOD system was exploited for 350 the development of buckypaper cathodes. One-pot  $\mathrm{BP}_{\mathrm{pp}}$  351 electrodes were first prepared then incubated with BOD, 352 washed with phosphate buffer at pH 7.0, then tested for 353 enzyme presence and activity. Figure 3A and B show CVs 354 f3 recorded in argon and oxygen at one-pot BP<sub>PP</sub>-BOD and BP- 355 BOD, respectively. Under oxygen, both types of electrode 356 exhibited similar onset potential of  $E_{\text{onset}}$  = 0.54  $\pm$  0.01 V vs 357 SCE and 0.52  $\pm$  0.01 V vs SCE, respectively. The onset 358 potentials are close to that of the predicted T1 copper site of 359 MvBOD responsible for substrate oxidation and successive 360 electron transfers  $(E_{1/2(T1)} = 0.48 \text{ V vs SCE at pH 7.0})$ .<sup>34</sup> The 361 onset potentials are close to the ideal thermodynamic reduction 362 potential for O<sub>2</sub> of 0.572 V vs SCE at pH 7.0 (assuming a 363 potential difference of 244 mV between RHE and SCE 364 reference electrodes). The onset potential values are therefore 365 very attractive for biofuel cell applications and consistent with 366 efficient single-proton single-electron DET between the BP and 367 the enzyme. 368

The catalytic wave observed in oxygen at BP<sub>PP</sub> confirms DET 369 accompanied by the electrocatalytic reduction of oxygen via 370



**Figure 3.** (A,B) CVs of bioelectrocatalytic O<sub>2</sub> reduction recorded at (A) BP<sub>PP</sub> (one-pot method) and (B) BP buckypaper electrodes after BOD enzyme immobilization in (--) Ar saturated and (-) O<sub>2</sub> saturated 0.1 mol L<sup>-1</sup> phosphate buffer at pH 7.0 at scan rate = 0.2 mV s<sup>-1</sup>. (C) Evolution of maximum catalytic current density as a function of time for BP<sub>PP</sub>-BOD. Chronoamperograms recorded at  $E_{app}$  = 0.2 V vs SCE and current densities obtained after 30 min. Error bars correspond to one standard deviation from two electrodes.

371 BOD. On the basis of repeat measurements, an average 372 maximum current density of  $0.34 \pm 0.15$  mA cm<sup>-2</sup> is observed 373 at BP compared to 1.33  $\pm$  0.17 mA cm<sup>-2</sup> for BP<sub>PP</sub> (one-pot 374 method), confirming substantially enhanced performance for 375 the protoporphyrin buckypaper. At BP, an ill-defined "residual slope" current is observed in oxygen, attributed to unfavorable 376 orientation of adsorbed enzymes. In contrast, at the BP<sub>PP</sub> 377 electrode, well-defined steady-state voltammograms are ob-378 served consistent with fast mass transport, enzyme catalysis, 379 and heterogeneous electron transfer at the buckypaper 380 electrode.<sup>37</sup> It is noted that a scan rate of 0.2 mV s<sup>-1</sup> was employed due to the superior steady-state signals with low 382 capacitance (see Figure S4 for catalytic currents recorded at 383 384 different scan rates). A summary of the catalytic parameters 385 obtained at different bioelectrodes is shown in Table 2.

Table 2. Catalytic Parameters for BP<sub>PP</sub>-BOD Cathode and BP<sub>PLQ</sub>-FADGDH Anode Prepared by One-Pot and Drop-Coating Functionalization Methods

buckypaper electrode (number <sup>a</sup> )	fabrication method (modifier concentration)	onset potential $(V)^b$	maximum catalytic current (mA cm <sup>-2</sup> ) <sup>b,c</sup>
$BP_{\rm PP}-BOD \\ (n = 5)$	one-pot (0.6 mmol $L^{-1}$ )	$0.54 \pm 0.01$	$1.33 \pm 0.17$
$BP_{\rm PP}-BOD \\ (n=3)$	drop-coat (0.6 mmol L <sup>-1</sup> )	$0.54 \pm 0.01$	$1.10 \pm 0.14$
$BP_{\rm PP}-BOD \\ (n=3)$	drop-coat (10 mmol $L^{-1}$ )	$0.54 \pm 0.01$	$1.26 \pm 0.11$
$\begin{array}{l} \text{BP-BOD}\\ (n=3) \end{array}$	unmodified	$0.52 \pm 0.01$	$0.34 \pm 0.15$
$BP_{PLQ} - FADGDH (n = 5)$	one-pot (2 mmol L <sup>-1</sup> )	$-0.23 \pm 0.01$	5.38 ± 0.54
$\begin{array}{l} \text{BP-FADGDH} \\ (n=2) \end{array}$	unmodified	$-0.01 \pm 0.00$	$0.002 \pm 0.001$

<sup>*a*</sup>Number of independent buckypaper electrode samples analyzed. <sup>*b*</sup>Parameters obtained from the forward sweep of CVs recorded at 0.2 mV s<sup>-1</sup>. <sup>*c*</sup>Current obtained at 0.2 and 0.15 V at BOD and FADGDH electrodes, respectively.

The long-term stability of BP<sub>pp</sub>-BOD was also assessed by periodically recording chronoamperograms at  $E_{app} = 0.2$  V vs SCE for 30 min over 24 days of storage in phosphate buffer at BP PT 7.0 (Figure S5). The corresponding plot in Figure 3C of the maximum catalytic current obtained on different days reveals remarkable stability for BP<sub>pp</sub>-BOD, with the current density decreasing by 10% over the first 7 days and 27% over 24 days. 392 Stability experiments performed in a similar manner at other 393 MWCNT-MCO enzyme cathodes report 40–45% current loss 394 after 1 week and 45–60% after 20–24 days.<sup>38,39</sup> To clarify, such 395 stability experiments evaluate both operational stability (for 30 396 min per day) and storage stability. The enhanced stability 397 observed here compared to that with CNT-modified GC 398 electrodes is consistent with improved physical enzyme 399 entrapment into the nanopore-containing CNT matrix via 400 fixation and/or dynamic reorganization effects.<sup>40</sup> 401

A brief assessment of the bioelectrocatalytic performance of 402 BP<sub>pp</sub>-BOD was also performed to demonstrate enzyme 403 inhibition at the biocathode. CVs recorded in the presence 404 and absence of 40 mmol L<sup>-1</sup> H<sub>2</sub>O<sub>2</sub> in phosphate buffer at pH 405 7.0 in oxygen are shown in Figure S6 and clearly reveal the loss 406 of oxygen reduction current due to inhibition of immobilized 407 bilirubin oxidase by  $H_2O_2$ . The catalytic current was suppressed 408 in the presence of H<sub>2</sub>O<sub>2</sub> and remained suppressed after transfer 409 to a fresh phosphate buffer solution, confirming that the 410 enzyme's activity was inhibited and not restored. The absence 411 of oxygen reduction in these experiments validates the 412 importance of the active "wired" enzyme as the biocatalyst. 413 Chronoamperometry performed at BP<sub>pp</sub>-BOD in phosphate 414 buffer at pH 7.0 in oxygen (Figure S6) revealed the rapid 415 nature of enzyme inhibition by H<sub>2</sub>O<sub>2</sub> and the good stability of 416 the biocathode in the presence of a physiologically relevant 417 concentration of NaCl (100 mM).

The bioelectrocatalytic performance of BP<sub>PP</sub> for oxygen 419 reduction was also performed at electrodes prepared by the 420 drop-coat method. No significant difference in  $E_{\text{onset}}$  was 421 observed between drop-coat and one-pot BP<sub>PP</sub> electrodes. 422 Likewise, equivalent sigmoidal steady-state current responses 423 (with different current magnitudes) were observed for all BP<sub>PP</sub> 424 electrodes. For drop-coat BP<sub>PP</sub>, the maximum average catalytic 425 current only slightly increased from  $1.10 \pm 0.14$  to  $1.26 \pm 0.11$  426 mA cm<sup>-2</sup> with an increase in protoporphyrin modifier from 0.6 427 mmol L<sup>-1</sup> to 10 mmol L<sup>-1</sup>.

The best performing biocathode identified here was the 429 BP<sub>pp</sub>-BOD prepared using the one-pot method with  $I_{\text{max}} = 1.33$  430  $\pm$  0.17 mA cm<sup>-2</sup>. The high performance of this biocathode is 431 clear given that typical values obtained by our group and others 432 for CNT paper-based MCO cathodes are 0.17 to 1.1 mA cm<sup>-2</sup> 433 in oxygen-saturated solution.<sup>27,29,30,41,42</sup> 434

Bioelectrocatalytic Glucose Oxidation at BPPLO Elec- 435 trodes with Immobilized FADGDH from Aspergillus sp. 436 For bioanode development, the one-pot method was exploited 437 for preparation of a new type of redox-embedded buckypaper 438 with immobilized FADGDH. To prepare the anode, a 439 MWCNT dispersion containing 2 mmol  $L^{-1}$  of 1,10-440 phenanthroline-5,6-dione (PLQ) was used. The bioanode was 441 obtained by drop-casting 150  $\mu$ L of 5 mg mL<sup>-1</sup> enzyme 442 solution onto the BP<sub>PLQ</sub> and leaving the solution overnight 443 until the droplet had fully adsorbed. The PLQ molecule has 444 previously been reported as a mediator for the cofactors 445 NADH/NADPH coupled with NAD/NADP-dependent en- 446 zymes.<sup>35,43</sup> To the best of our knowledge, the phenanthroline 447 quinone as a free ligand has not been demonstrated as a 448 mediator for FAD-dependent enzymes such as FADGDH. In 449 addition to the low redox potentials, a major advantage of 450 phenanthroline quinone mediators is their nonreactivity toward 451 active-site enzyme amine and thiol groups.<sup>43</sup> In this work, we 452 have investigated the use of PLQ, in the form of a redox- 453 embedded functionalized buckypaper, to electrically connect 454



**Figure 4.** (A) Scheme illustrating bioelectrocatalytic oxidation of glucose on  $BP_{PLQ}$  buckypaper via MET with the active site of FADGDH. (B) CVs recorded at a  $BP_{PLQ}$  buckypaper electrode after FADGDH immobilization in (--) 0 mmol L<sup>-1</sup> and (--) 170 mmol L<sup>-1</sup> glucose in Ar saturated McIlvaine buffer at pH 7.0 at scan rate = 0.2 mV s<sup>-1</sup>. (C) Plot of average current density obtained for different glucose concentrations recorded at three  $BP_{PLQ}$ -FADGDH electrodes. (D) Evolution of maximum catalytic current density as a function of time for  $BP_{PLQ}$ -FADGDH with 170 mmol L<sup>-1</sup> glucose. (C, D) Chronoamperograms recorded at  $E_{app} = 0.15$  V vs SCE and current densities obtained after 30 min. Error bars correspond to one standard deviation from at least two electrodes.

455 the active site of FADGDH to the electrode for bioelec-456 trocatalytic oxidation of glucose (see Figure 4A). In this 457 mechanism, the FADGDH oxidizes the  $\beta$ -D-glucose to D-458 glucono-1,5-lactone using the FAD cofactor, which itself is 459 reduced to FADH<sub>2</sub>. The PLQ mediator then acts as a 460 secondary electron acceptor to oxidize the reduced cofactor, 461 FADH<sub>2</sub>. The mediator is finally reoxidized by the electrode 462 which is set at an appropriate oxidizing potential.

Figure 4B and Figure S7 show CVs recorded in 0 (--) and 463 464 170 mmol  $L^{-1}$  (-) glucose in McIlvaine buffer at pH 7.0 at 465 one-pot BP<sub>PLQ</sub>-FADGDH and BP-FADGDH electrodes, 466 respectively. In the presence of 170 mmol  $L^{-1}$  glucose, an 467 onset potential of  $E_{\text{onset}} = -0.23 \pm 0.01$  V vs SCE is observed at 468  $BP_{PLQ}$ -FADGDH, which is attractively low for a glucose-469 oxidizing bioanode and similar to that obtained using 1,4 469 on aphthoquinone hydrogel mediators with FADGDH ( $E_{onset} = 10^{-1} - 10^{-22/23}$ -0.18 to -0.25 V vs SCE at near neutral pH). 471 472 Interestingly, the onset potential of -0.23 V is much more 473 negative than the  $\approx$ -0.05 V previously reported using a Ru-474 PLQ polymer with FADGDH,<sup>20</sup> highlighting an advantage of 475 using the free PLQ mediator in this form. The onset potential is 476 around 180 mV positive of the estimated redox potential of 477 -0.41 V vs SCE for the enzyme-bound relay, FAD/FADH<sub>2</sub>, consistent with thermodynamically attractive electron wiring. 478 479 The onset potential at  $BP_{PLQ}$  for glucose oxidation is also about 480 200 mV more negative than ferrocene and osmium mediator-<sup>481</sup> modified electrodes with  $E_{\text{onset}} \approx -0.05$  to 0.15 V vs <sup>482</sup> SCE, <sup>17,19,21</sup> and thus PLQ is an attractive mediator for biofuel 483 cell applications.

<sup>484</sup> The voltammograms recorded at  $BP_{PLQ}$  under argon in the <sup>485</sup> absence and presence of 170 mmol  $L^{-1}$  glucose clearly 486 demonstrate a drastic increase in current signal with glucose 487 addition. Well-defined sigmoidal waves are observed at 0.2 mV 488 s<sup>-1</sup> consistent with electrocatalytic oxidation of glucose. A 489 maximum current density of 5.38  $\pm$  0.54 mA cm<sup>-2</sup> is observed 490 at 0.15 V at BP<sub>PLQ</sub> without stirring. In contrast, voltammograms 491 recorded at BP under the same conditions reveal a negligible 492 maximum current density of 0.002  $\pm$  0.001 mA cm<sup>-2</sup>. The 493 substantial enhancement in catalytic current provides compel-494 ling evidence for mediated electron transfer reaction via PLQ. 495 The high catalytic currents obtained were subsequently 496 validated by comparison with a CNT paper prepared using a 497 known mediator for FADGDH. A 1,4 naphthoquinone 498 buckypaper, BP<sub>NQ</sub>-FADGDH, was prepared and tested in the 499 same manner as for BP<sub>PLQ</sub>-FADGDH. Voltammetry revealed a 500 significantly smaller maximum current density of 2.20 mA cm<sup>-2</sup> 501 (Figure S8). Despite being less powerful than the  $BP_{PLO}$  electrode, the  $BP_{NQ}$  electrode still exceeds recent high  $_{502}$  performance NQ-anodes.  $^{22,23}$   $_{503}$ 

The catalytic current obtained of 5.38  $\pm$  0.54 mA cm<sup>-2</sup> at 504 0.15 V vs SCE for BPPLO in unstirred solution exceeds the 505 performance of that observed at most bioanodes to date 506 without the use of hydrodynamic conditions. We believe that 507 the BP<sub>PLQ</sub> anode exhibits the highest catalytic density for 508 glucose oxidation of any paper-based bioanode. At phenothia- 509 zine-modified commercial buckypaper with immobilized NAD- 510 dependent GDH and NAD cofactor, current densities up to 2.6 511 mÅ cm<sup>-2</sup> at 25 °C have been reported.<sup>25</sup> With the addition of 1 512 mmol L<sup>-1</sup> NAD<sup>+</sup> in solution, the catalytic current increased to 513 4.5 mA cm<sup>-2</sup> at a high potential of 0.35 V. In addition to the 514 high potential required, the use of NAD in solution is less 515 convenient than if the cofactor is surface-bound or enzyme- 516 bound. High performing bioanode architectures typically  $_{517}$  produce no more than 2 mA cm<sup>-2 22,44,45</sup> with the exception  $_{518}$ of a hierarchical porous carbon bioelectrode which exibited 519 enormous densities up to 100 mA cm<sup>-2</sup> with rapid 520 convection.<sup>18</sup> With CNT-modified Toray papers with immo- 521 bilized glucose oxidase and dehydrogenases, current densities in 522 the range 1-3.3 mA cm<sup>-2</sup> have been reported.<sup>23,46-48</sup> 523

Evaluation of the steady-state current at a fixed potential of 524 0.15 V as a function of glucose concentration reveals a linear 525 increase in the range 1 mmol  $L^{-1}$  to 50 mmol  $L^{-1}$  (see 526 calibration plot in Figure S9). As a side note, the linearity of  $r^2$  527 = 0.996 and the ability to detect beyond the upper limit of 30 528 mmol  $L^{-1}$  means that the BP<sub>PLQ</sub>-FADGDH meets basic 529 requirements for a commercial glucose sensor. 530

Figure 4C shows that the steady-state currents increased with 531 increasing concentration to a plateau at 170 mmol  $L^{-1}$  glucose; 532 hence 170 mmol  $L^{-1}$  was adopted in experiments as the 533 concentration to maximize catalytic current output, limited by 534 the enzymatic reaction and catalyst surface coverage. Limiting 535 current values were reached within 30 s (Figure S10), 536 consistent with fast mass transport of glucose at the electrode. 537 Estimated values for the apparent Michaelis–Menten and 538 velocity constants of  $K_{\rm m} = 40.4$  mmol  $L^{-1}$  and  $V_{\rm max} = 6.1$  mA 539 cm<sup>-2</sup>, respectively, are obtained. The estimated  $K_{\rm m}$  is similar to 540 that observed for fungal FADGDHs ( $K_{\rm m} = 35$  mmol  $L^{-149}$ ), 541 and hence the BP<sub>PLQ</sub> electrode maximizes electrocatalysis 542 without significantly affecting the enzymes' binding constant for 543 glucose.

The stability of the BP<sub>PLQ</sub>-FADGDH bioanode was assessed 545 over 10 days by periodically recording chronoamperograms at 546  $E_{app}$  = 0.15 V vs SCE for 30 min in McIlvaine buffer at pH 7.0 547 (Figure S11). The plot in Figure 4D of the maximum catalytic 548

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s49 current obtained on different days reveals that the bioanode is s50 significantly less stable than the biocathode. After 2 days, 75% s51 of the original current remains. After 5 days, only 48% of the s52 initial current remains. Similar storage stability for an s53 FADGDH electrode has previously been observed using an s54 Os polymer mediator with 80% of the initial current observed s55 after 2 days followed by a rapid breakdown to 56% after 6 s56 days.<sup>13</sup> This finding suggests that PLQ may be no less toxic or s57 inhibitory toward FADGDH than osmium polymers. Despite s58 the poor stability, high maximum current densities of  $\approx 1$  mA s59 cm<sup>-2</sup> are nevertheless possible after 10 days, confirming that s60 the BP<sub>PLQ</sub> is operational for several days.

Assessment of the bioelectrocatalytic performance of BP<sub>PLO</sub>-561 562 FADGDH was also performed to explore enzyme inhibition at 563 the bioanode. CVs recorded before and after the addition of 10 mmol  $L^{-1}$  of CuCl<sub>2</sub> in McIlvaine buffer at pH 7.0 are shown in 564 Figure S12 and clearly reveal the loss of glucose oxidation 565 current due to inhibition of immobilized FADGDH, attributed 566 to binding of  $Cu^{2+}$  to the FADH<sub>2</sub> cofactor as previously 567 568 observed for glucose oxidase.<sup>50</sup> The possibility to reverse the 569 enzyme inhibition by addition of a strong metal chelator to 570 reverse binding of the metal ions to FAD was also tested. The 571 voltammogram obtained after addition of an excess of 572 ethylenediaminetetracetic acid (EDTA, 11 mmol  $L^{-1}$ ) and 573 mild stirring shows an increase in the catalytic oxidation current 574 on the reverse sweep, attributed to partial reactivation of the biocatalyst. 575

Single Compartment Biofuel Cell with a BP<sub>PP</sub>-BOD S77 Cathode and BP<sub>PLQ</sub>-FADGDH Anode Prepared via One-S78 Pot Fabrication. Power generation from membraneless S79 glucose/oxygen biofuel cells using redox-embedded buckys80 papers was subsequently investigated. A single-compartment S81 glucose/O<sub>2</sub> paper-based biofuel cell was constructed using a S82 BP<sub>PP</sub>-BOD cathode and a BP<sub>PLQ</sub>-FADGDH anode prepared via S83 one-pot methods (Figure SA). Linear polarization curves were



**Figure 5.** (A) Scheme illustrating the single compartment buckypaper biofuel cell comprising an O<sub>2</sub> reducing BP<sub>PP</sub>-BOD cathode and glucose oxidizing BP<sub>PLQ</sub>-FADGDH anode. (B, C) Biofuel cell polarization (---) and power curves (-) recorded under (B) oxygen-saturated and (C) quiescent oxygen conditions in McIlvaine buffer at pH 7.0 with 170 mmol L<sup>-1</sup> glucose. Polarization voltammograms were recorded at 0.2 mV s<sup>-1</sup>. Error bars correspond to one standard deviation from three biofuel cells.

recorded at 0.2 mV s<sup>-1</sup> in McIlvaine buffer at pH 7.0 to evaluate 584 the performance under oxygen-saturated ( $\approx 1.1 \text{ mmol L}^{-1}$ ) and 585 quiescent oxygen conditions ( $\approx 0.23 \text{ mmol L}^{-1}$ ) with 170 586 mmol L<sup>-1</sup> glucose.<sup>51</sup> Large OCVs of 0.74  $\pm$  0.01 V and 0.67  $\pm$  587 0.01 V were obtained under quiescent and oxygen-saturated 588 conditions, respectively. The OCVs match closely the estimated 589 maximum voltage of 0.77 V from the half-cell polarization 590 experiments. The difference in OCV between the quiescent and 591 oxygen-saturated conditions is attributed to a small amount of 592 degradation between fuel cell testing experiments. 593

Average polarization and power curves (Figure 5B and C) 594 reveal a maximum power density of 0.65  $\pm$  0.10 mW cm<sup>-2</sup> or 595 24.07 mW cm<sup>-3</sup> at 0.5 V for the biofuel cell under oxygen- 596 saturated conditions without stirring. Under quiescent oxygen 597 with no stirring, a maximum power density of 0.053 mW cm<sup>-2</sup> 598 or 1.97 mW cm<sup>-3</sup> is observed. The power outputs for these 599 glucose/O2 biofuel cells are either very good or exceptional 600 depending on whether the power delivery is divided by the 601 surface area  $(cm^2)$  or volume  $(cm^3)$ . It is noted that we used 602 equal sized anodes and cathodes in this work and that the 603 power densities were obtained by dividing the power delivery 604 by either the surface area or volume of one electrode. Given 605 that buckypaper is a three-dimensional electrode and size is a 606 crucial parameter for portable biofuel cell applications, the 607 power density in mW cm<sup>-3</sup> is arguably more appropriate. 608 However, for this work we have chosen to remain with the 609 standard mW cm<sup>-2</sup> convention for figures. Maximum power 610 outputs for a single EBFC in the literature are between 1.45 and 611 2.3 mW cm<sup>-2</sup> at 0.3 to 0.55 V.<sup>22,23,52</sup> One of these previously <sub>612</sub> reported biofuel cells, based on our estimates, gives up to  $3.8_{613}$  mW cm<sup>-3</sup> (1.54 mW cm<sup>-2 52</sup>), and thus the delivery of 24.07 614 mW cm<sup>-3</sup> reported here is markedly high. 615

The difference in power density observed between the 616 saturated and quiescent oxygen conditions reveals that the 617 biofuel cell is strongly limited by oxygen availability at the 618 cathode. Even in the presence of oxygen-saturated conditions, 619 the biocathode is limiting. 620

Polarization and power curves were also recorded at freshly  $_{621}$  prepared biofuel cells in the absence of glucose under oxygen-  $_{622}$  saturated conditions as control experiments (Figure S13). In  $_{623}$  the absence of the enzyme's substrate, the low power output  $_{624}$  and a small OCV, namely 0.02 mW cm<sup>-2</sup> and 0.53  $\pm$  0.02 V,  $_{625}$  clearly illustrate and confirm the unambiguous role of  $_{626}$  FADGDH and the need for glucose for effective biofuel cell  $_{627}$  performance.

In order to assess the operational stability of the biofuel cell, 629 potentiostatic and galvanostatic tests were performed for 30 630 min. This duration may, for example, be considered as an 631 adequate operational time for a single use self-powered 632 biosensor. The stability of the biofuel cell was first examined 633 by applying a mild fixed voltage of 0.2 V and monitoring the 634 current in oxygen-saturated solution. The power obtained from 635 the recorded current revealed a stable power output of 295  $\pm$  636 25  $\mu$ W cm<sup>-2</sup> after an initial 30 s induction period (Figure 6A). 637 f6 Similar glucose/oxygen biofuel cell stability has been observed 638 using FADGDH, which, notably, is vastly superior to that 639 observed with the GOx enzyme.<sup>14</sup> The initial induction period 640 is attributed to diffusional equilibration and high charging 641 currents. To further assess the stability, a current of 500  $\mu$ A was 642 continuously drawn and the evolution of voltage monitored 643 (Figure 6B). Following the short initial induction period, a 644 stable voltage of  $0.57 \pm 0.01$  V is obtained. 645



**Figure 6.** (A) Power generated from current discharge at 0.2 V and (B) voltage generated at 600  $\mu$ A cm<sup>-2</sup> (500  $\mu$ A) for 30 min operation of the BP<sub>PP</sub>-BOD/BP<sub>PLQ</sub>-FADGDH biofuel cell in O<sub>2</sub> saturated McIlvaine buffer at pH 7.0 with 170 mmol L<sup>-1</sup> glucose. Error bars correspond to one standard deviation from three biofuel cells.

#### 646 CONCLUSIONS

647 Electricity generation from glucose and oxygen using small and 648 lightweight enzymatic biofuel cells opens up the attractive 649 prospect of self-powered health and environmental sensor 650 devices. Here, we report the fabrication of new freestanding 651 redox-embedded (porphyrin, phenanthroline quinone, and 652 napthoquinone) carbon nanotube paper electrodes with 653 physical durability, practical flexibility, and excellent electro-654 chemical properties. Elaboration of the electrodes for 655 construction of bioelectrodes with high catalytic performance 656 compared to literature values was subsequently demonstrated. 657 Very high catalytic performance was observed by employing 658 1,10-phenanthroline-5,6-dione as an electron transfer mediator 659 with FADGDH at the anode. The biofuel cell delivers milliwatt 660 per cubic centimeter power densities under either quiescent 661 solution (dissolved oxygen) or saturated oxygen solution  $_{\rm 662}$  conditions, with 170 mmol  $L^{-1}$  glucose at neutral pH and 663 room temperature. In addition, the half-cell and biofuel cell 664 experiments show good operational stability, which could be 665 appropriate for disposable self-powered sensors. We expect that 666 the proposed fabrication methods, buckypapers, and use of 667 PLQ for mediated electron transfer with FADGDH will 668 advance the field of biofuel cells toward practical applications, 669 especially considering the excellent prospects of the FADGDH 670 enzyme and paper-based bioelectrodes. Future work is now 671 required to address the limiting cathode power output under 672 quiescent oxygen levels (for example, by enhancement of 673 dioxygen mass transport) and the comparatively poor stability 674 observed at the anode over several days (for example, via caging 675 and shrinking effects).

### 676 ASSOCIATED CONTENT

#### 677 **Supporting Information**

678 The Supporting Information is available free of charge on the 679 ACS Publications website at DOI: 10.1021/acscatal.7b00738.

Electrode characterization and stability, Figures S1–S13(PDF)

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